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Laser-driven ion sources for medical radioisotope generation

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Arianna Formenti¹, Andrea Pazzaglia¹, Luca Fedeli³, Matteo Passoni¹

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Laser-driven ion sources for medical radioisotope generation

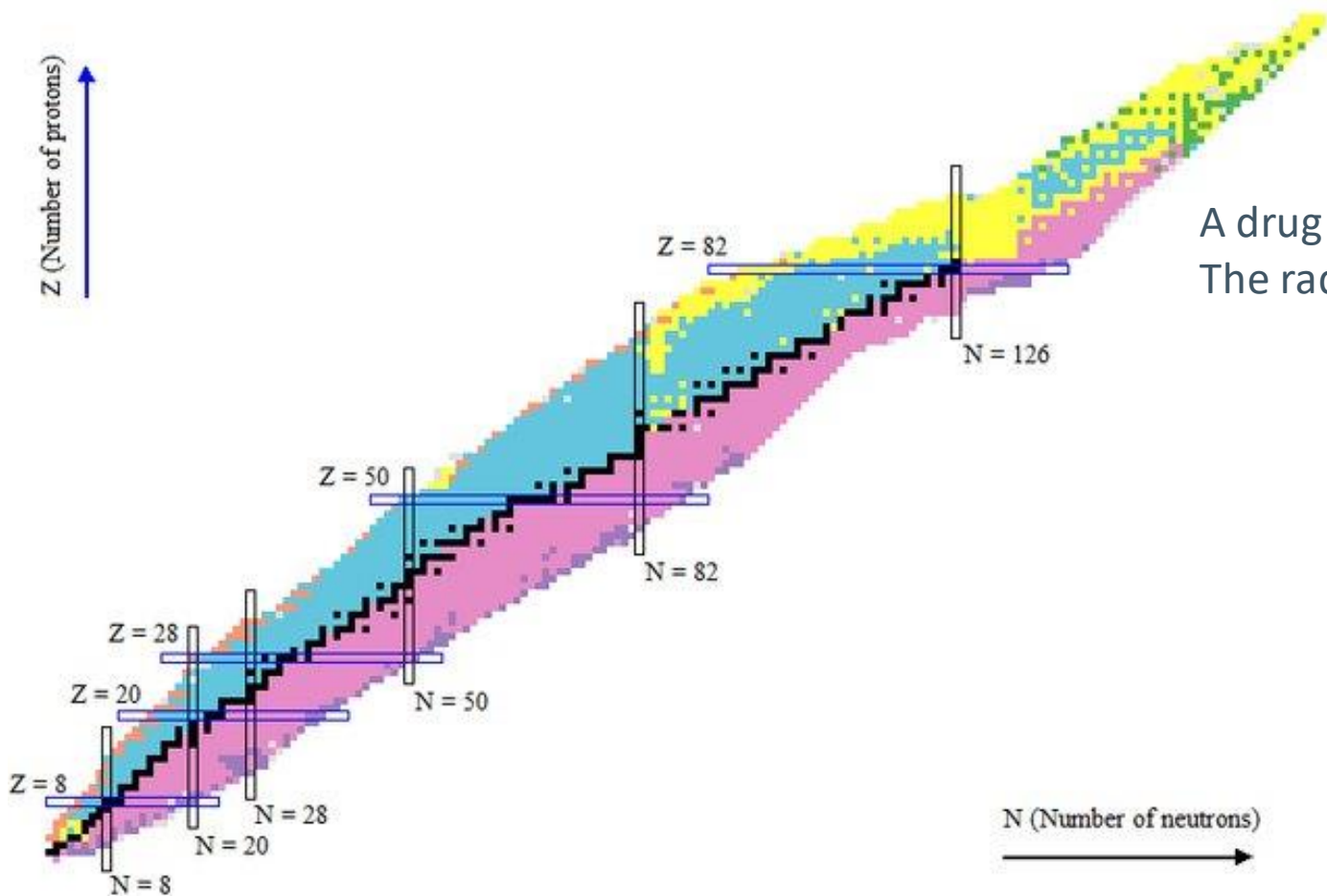


Laser-driven ion sources for **medical radioisotope** generation



Radioisotopes in Nuclear Medicine

Application of radioisotopes for the diagnosis and treatment of diseases.

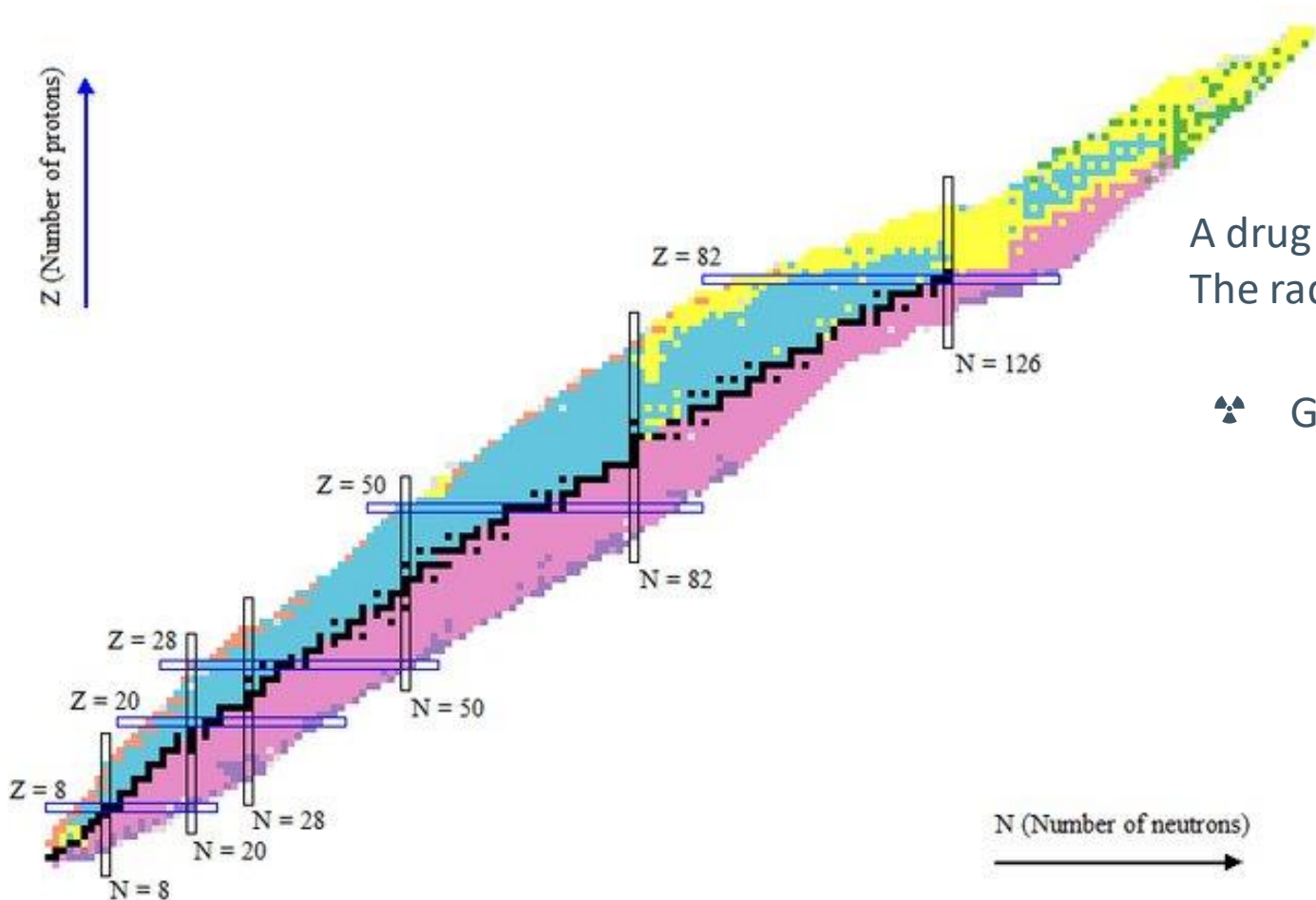


A drug delivers radionuclides to biological target sites
The radioactive decay is exploited to:



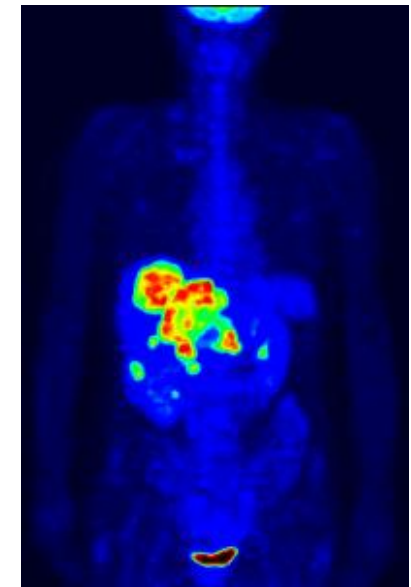
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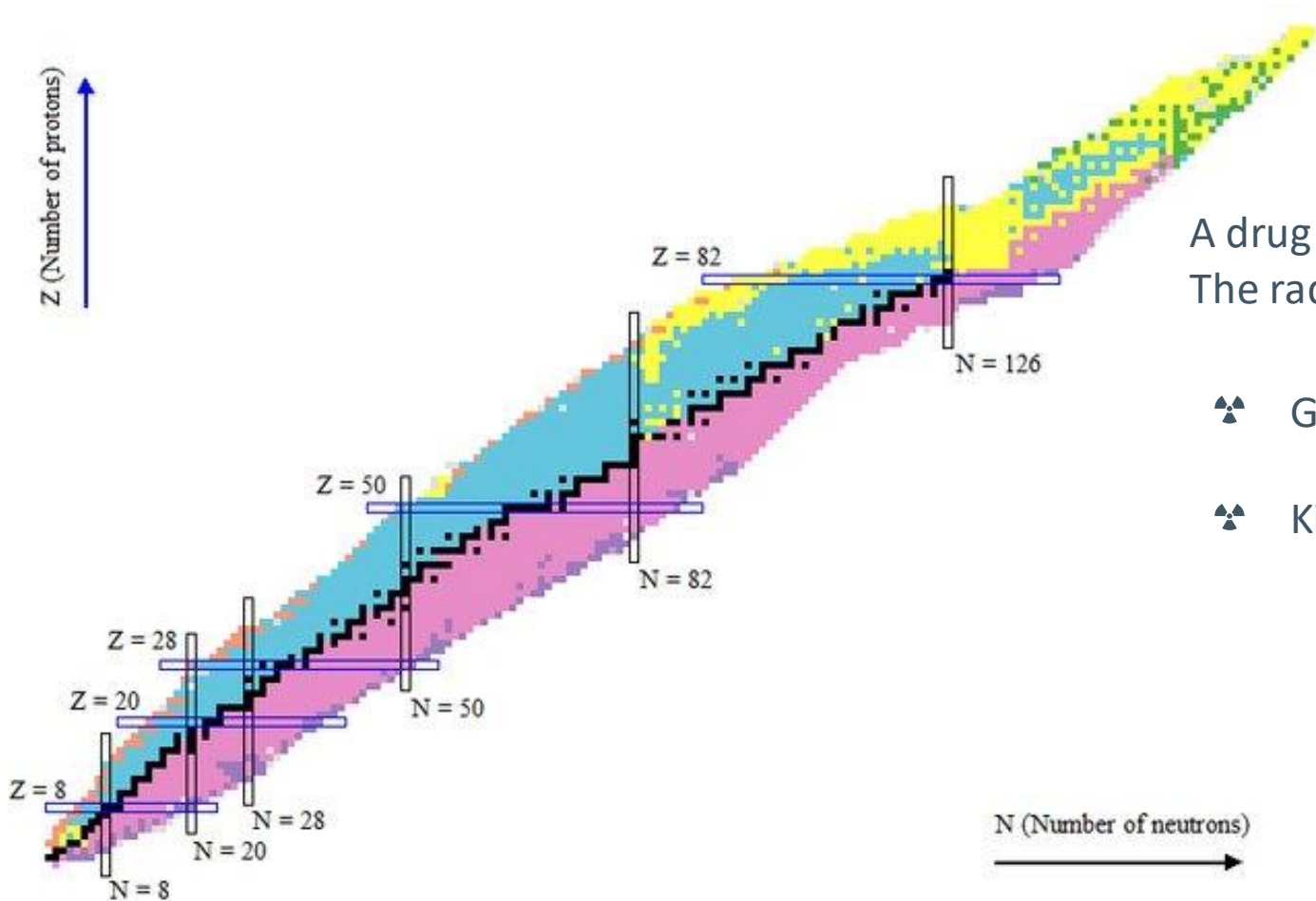
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The radioactive decay is exploited to:

- ☢ Gather **anatomical** and **functional** information



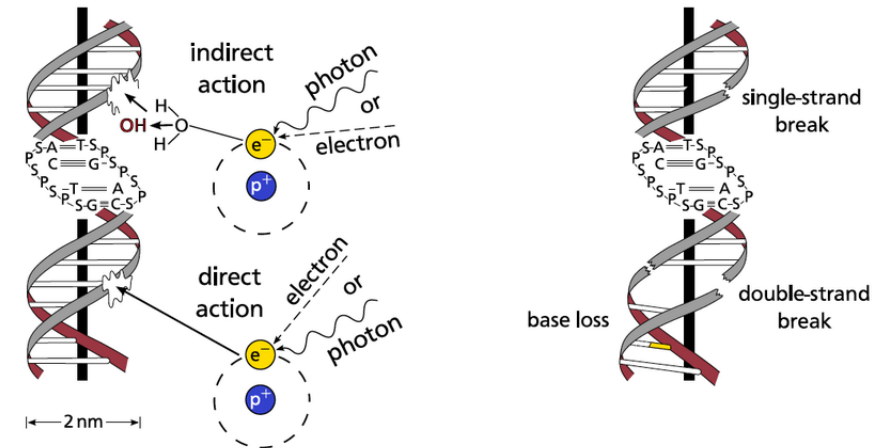
Radioisotopes in Nuclear Medicine

Application of radioisotopes for the diagnosis and **treatment** of diseases.



A drug delivers radionuclides to biological target sites
The radioactive decay is exploited to:

- ☢ Gather **anatomical** and **functional** information
- ☢ Kill malignant cells breaking their **DNA**

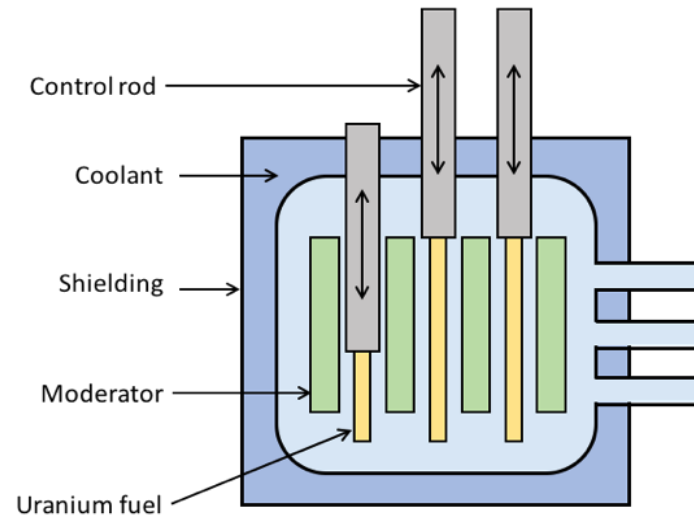


Production of medical radionuclides

Radionuclides decay: cannot be stored indefinitely. Constant production is required, even *in situ*

Nuclear fission reactors

$$\Phi = 10^{10} \div 10^{16} \text{ neutrons/cm}^2 \cdot \text{s}$$



^{99m}Tc used in 80% of nuclear diagnostics exams

^{133}I treating and imaging of thyroid

^{133}Xe - lung studies, half-life 5 days

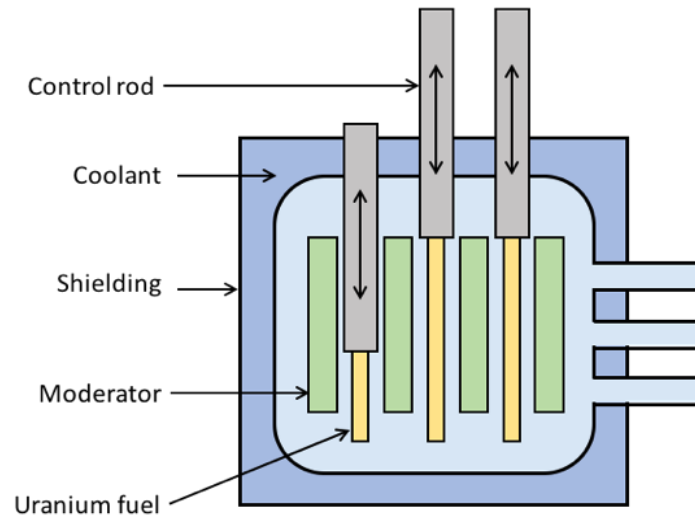


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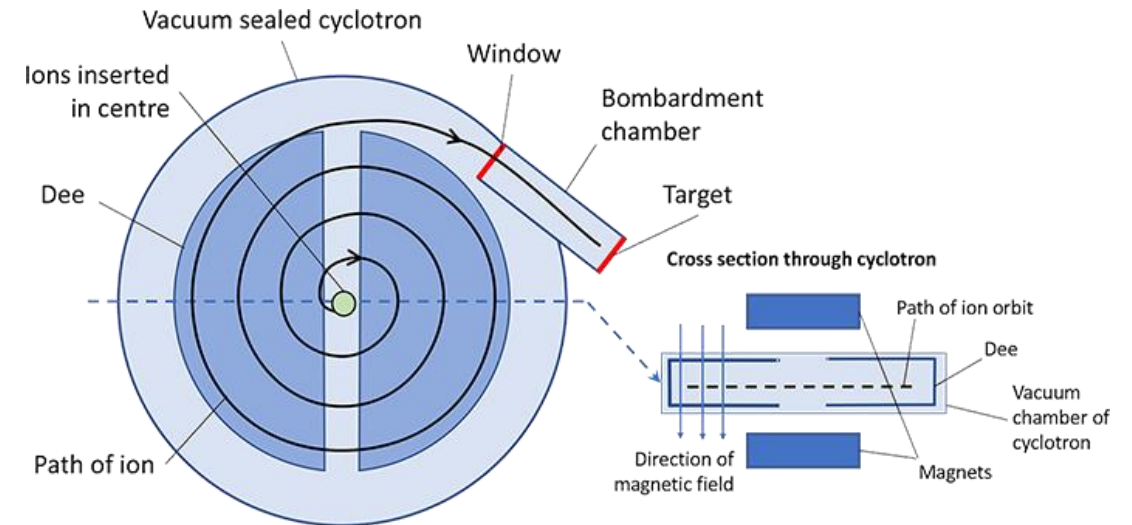
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Conventional accelerators (mainly cyclotrons)



^{18}F for PET scanning (half-life 1.87 hours)
 ^{67}Ga for imaging of inflammation / tumors
 ^{81m}Kr for lung studies (half-life 13 s!)



PARTICLE ACCELERATORS

CONVENTIONAL

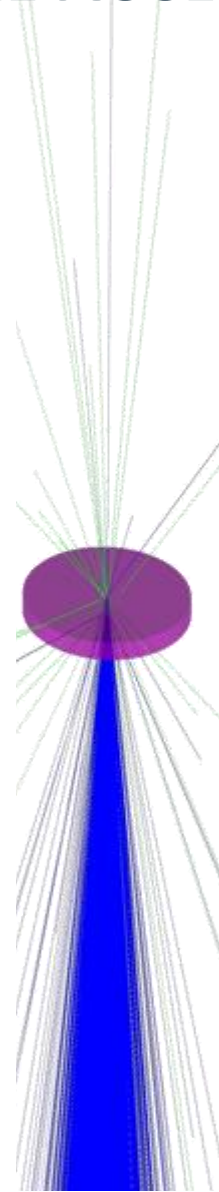
The current state of the art is the **CYCLOTRON**

PROS

- ❖ High current: 10 – 100 μA
- ❖ High energy: 10 - 30 MeV
- ❖ High activity produced

CONS

- ❖ Neutron – gamma flux:
Activation of the component,
Shielding, Waste
- ❖ Dimension and costs
- ❖ Limited versatility:
particles and energy are
difficult to change



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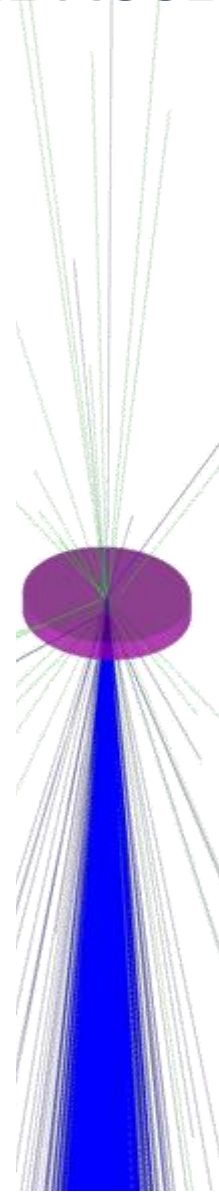
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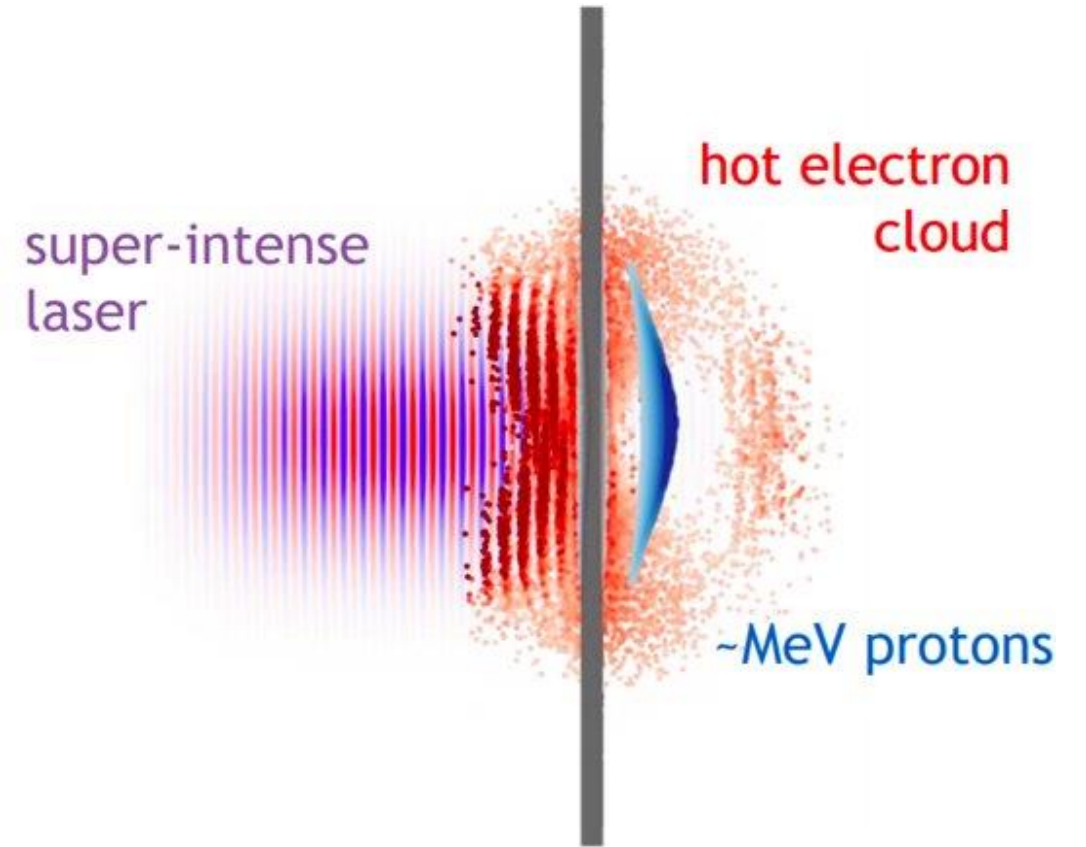
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LASER-DRIVEN



Potential for **flexibility** and cost **reduction!**

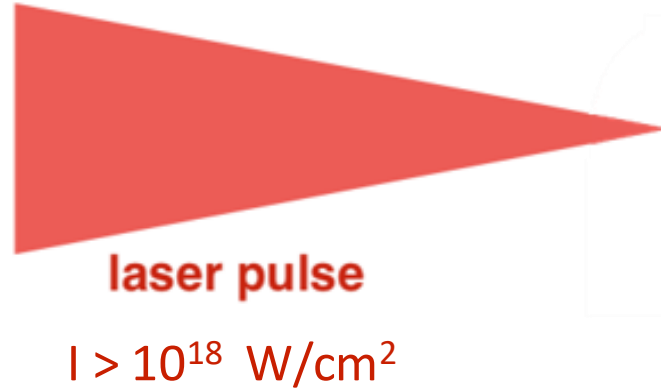
A. Macchi et al., Rev. Mod. Phys. 85, 751 (2013)



Laser-driven ion sources for medical radioisotope generation



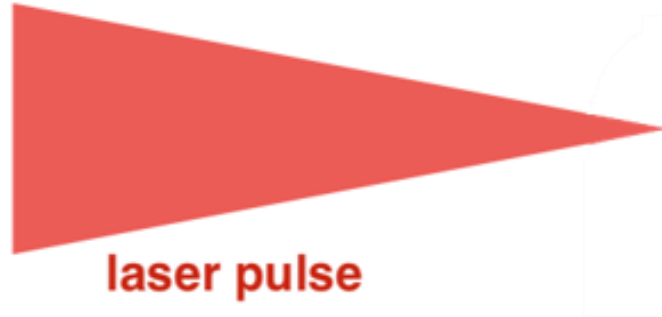
Laser-Driven Particle Acceleration



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Laser-Driven Particle Acceleration



$I > 10^{18} \text{ W/cm}^2$

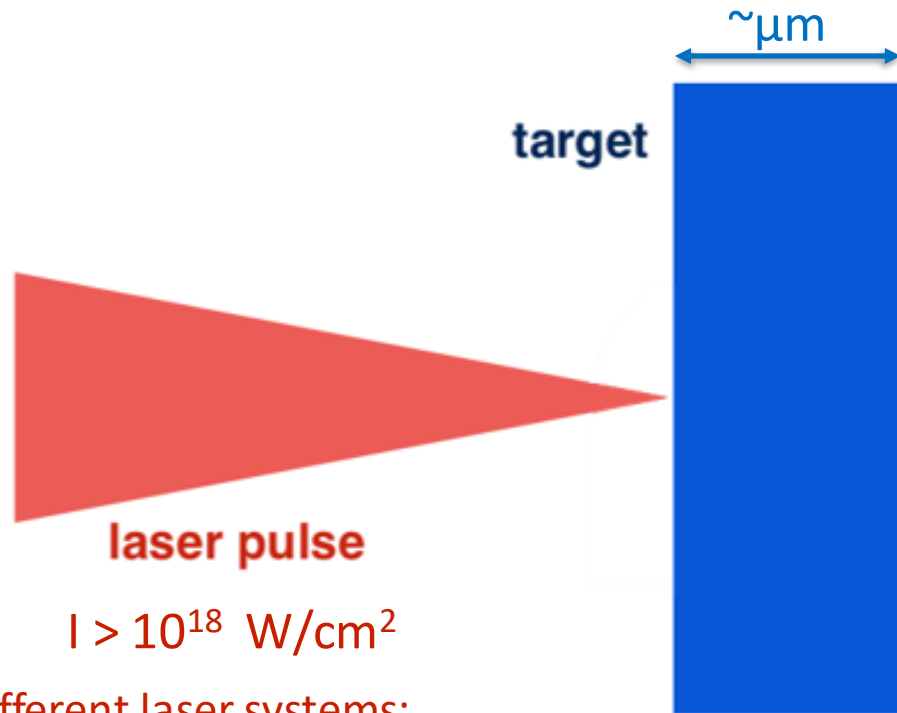
Different laser systems:

- ❖ 0.1-10 J, 30 fs, high rep rate(compact)
- ❖ 10 J-1 kJ, ps, low rep rate (large)

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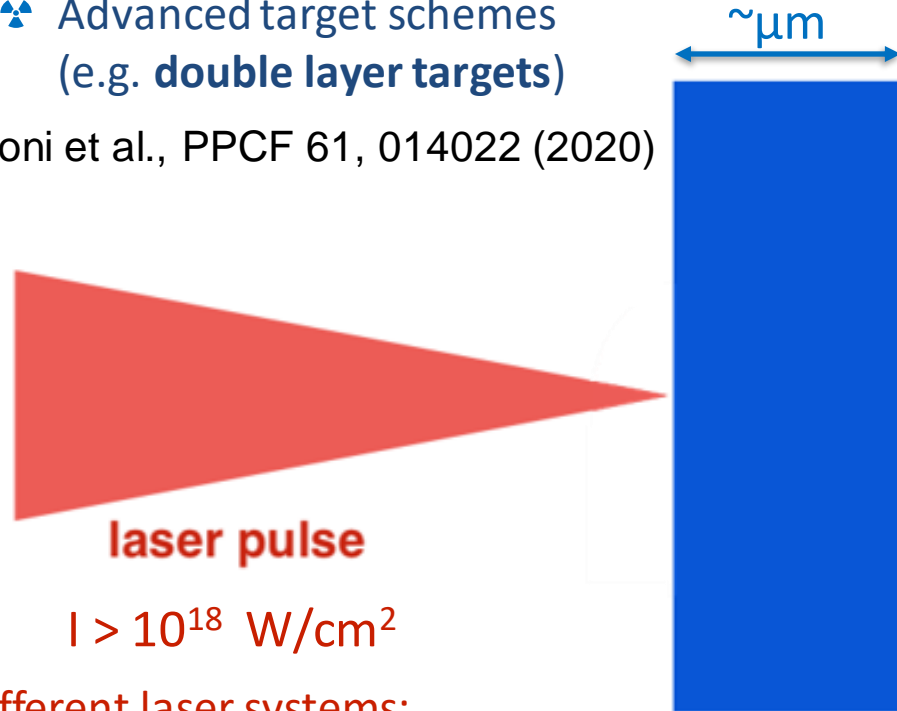


Laser-Driven Particle Acceleration

Different target concepts:

- ❖ Simple micrometric foil
- ❖ Advanced target schemes (e.g. **double layer targets**)

M. Passoni et al., PPCF 61, 014022 (2020)



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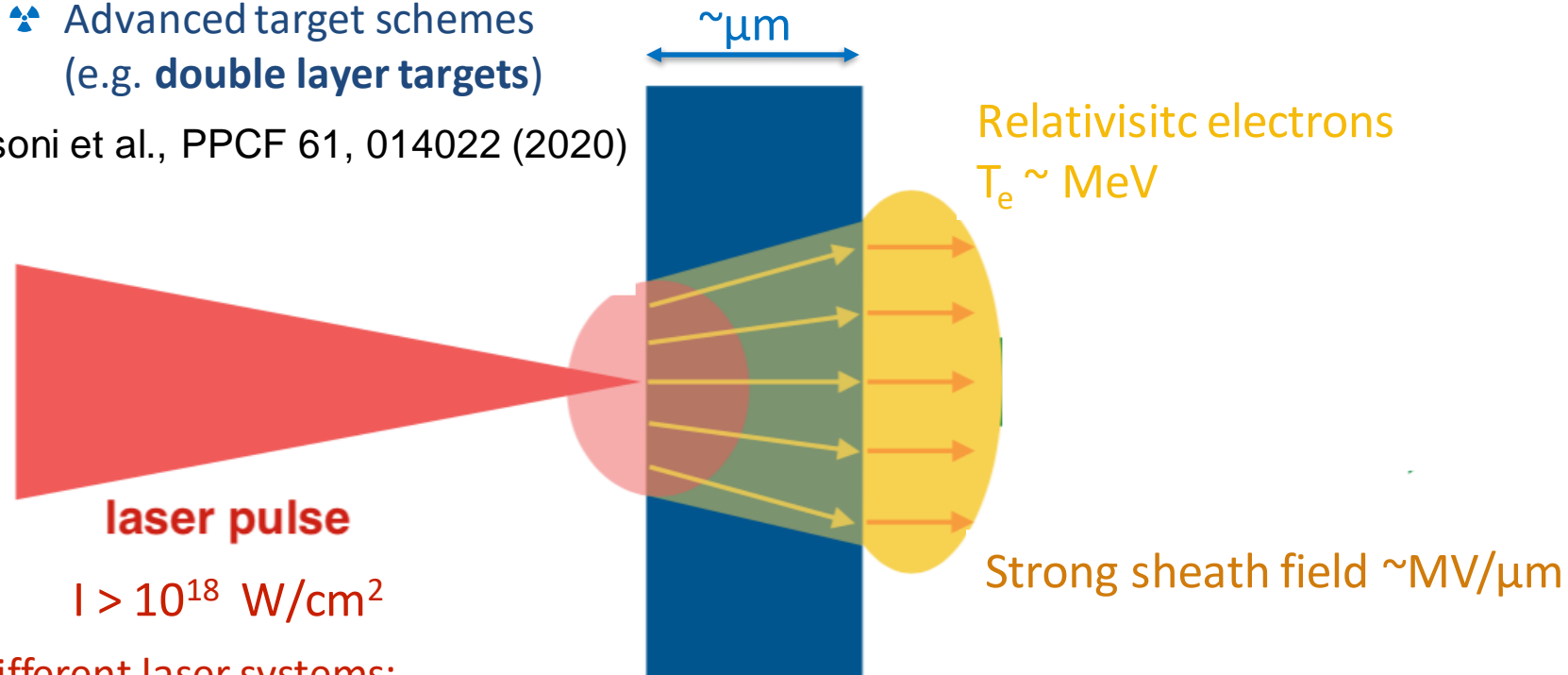


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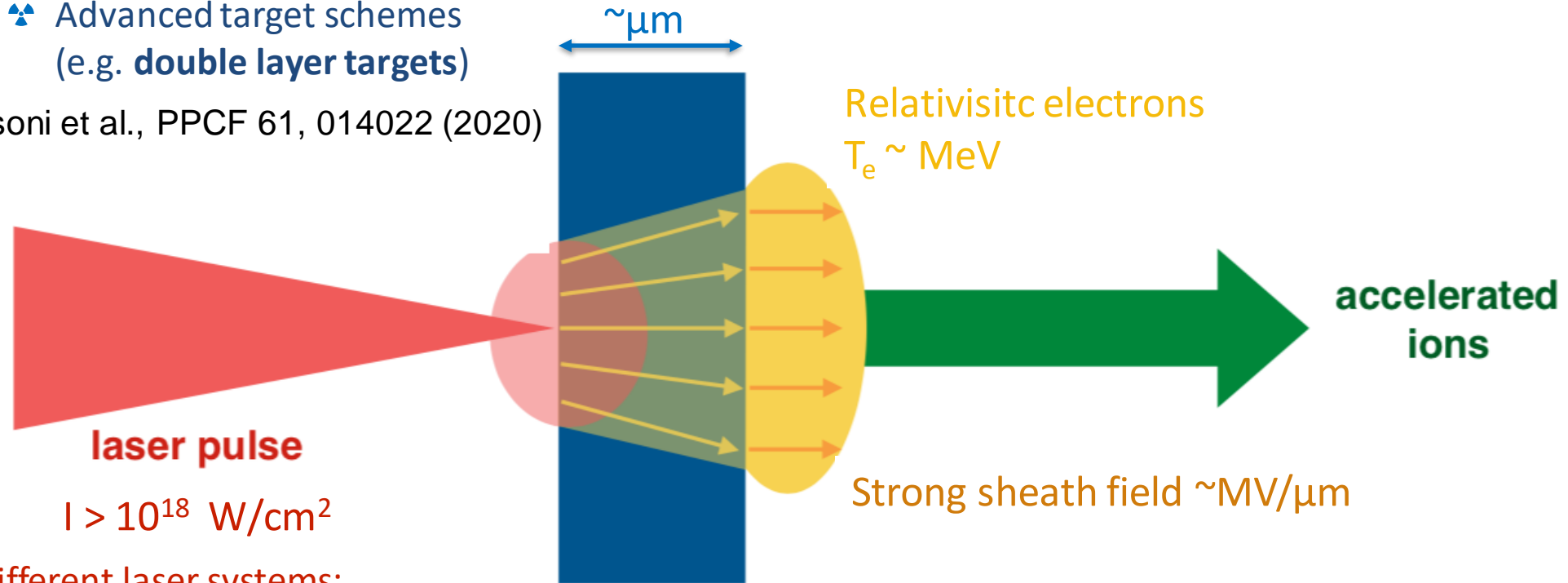


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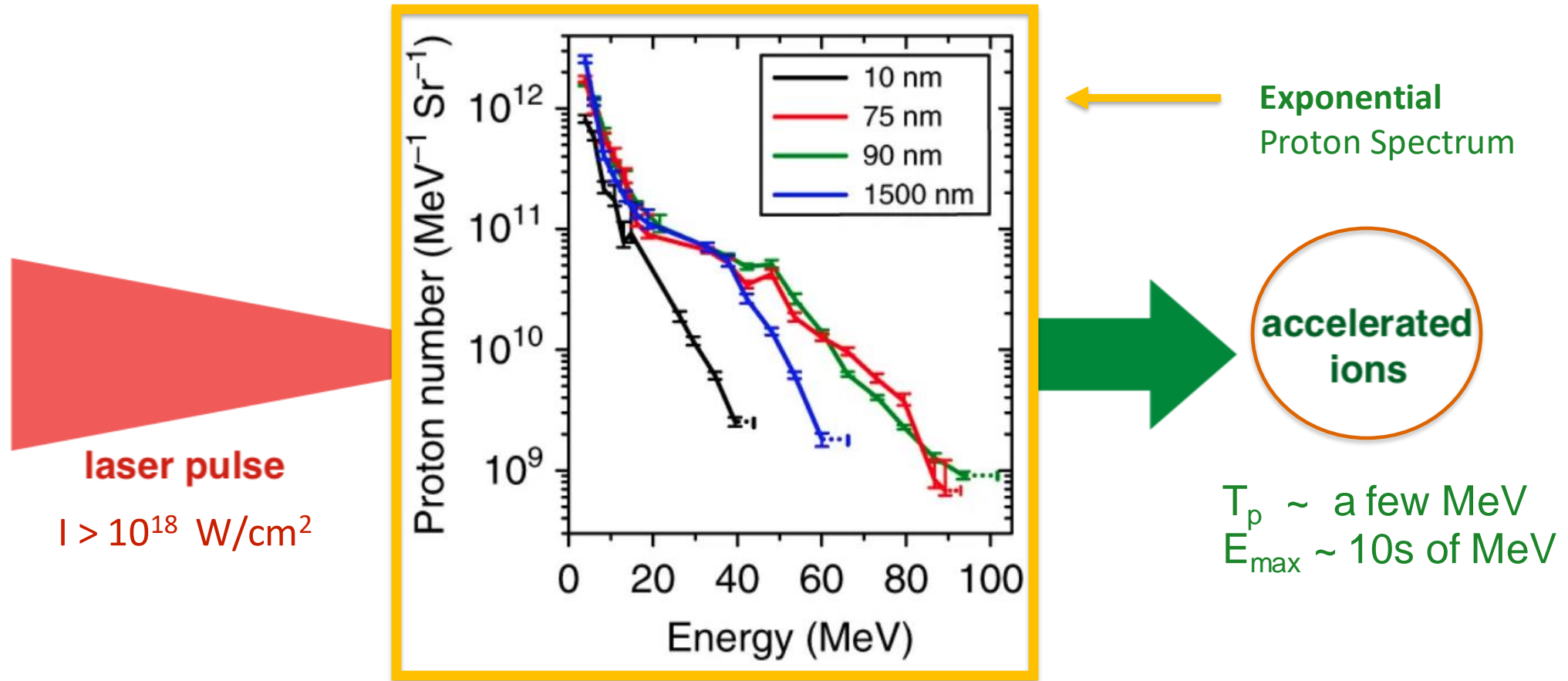
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A. Macchi et al., Rev. Mod. Phys. 85, 751 (2013)



Target Normal Sheath Acceleration



A. Higginson et al., Nature Comm. 9, 724 (2018)

Laser-driven ion sources for medical **radioisotope generation**



A few works in literature which use laser-driven accelerators to produce radioisotopes....

Experimental

- ❖ S. Fritzier, V. Malka, G. Grillon, J. P. Rousseau et al.
Proton beams generated with high-intensity lasers: Applications to medical isotope production.
Applied Physics Letters, 2003.
- ❖ K.W.D. Ledingham, P. McKenna, T. McCanny, S. Shimizu et al.
High power laser production of short-lived isotopes for positron emission tomography.
Journal of Physics D: Applied Physics, 2004.
- ❖ I. Spencer, K.W.D. Ledingham, R. P. Singhal, T. McCanny et al.
Laser generation of proton beams for the production of short-lived positron emitting radioisotopes.
Nuclear Instruments and Methods in Physics Research, 2001.

TW - laser
 E_{\max} 10 MeV
 $^{11}\text{B} (p,n) ^{11}\text{C}$

PW - laser
 E_{\max} 30 MeV
 $^{18}\text{O} (p,n) ^{18}\text{F}$

PW - laser
 E_{\max} 37 MeV
 $^{18}\text{O} (p,n) ^{18}\text{F}$

Theoretical

- ❖ A. Italiano, E. Amato, F. Minutoli, D. Margarone et al.
Production of ^{68}Ge , ^{64}Cu , ^{86}Y , ^{89}Zr , ^{73}Se , ^{77}Br and ^{124}I positron emitting radionuclides through future laser-accelerated proton beams at Eli-Beamlines for innovative PET diagnostics, 2016

PW - laser
TALYS code

A.J. Koning et al., AIP Conference Proceedings 769, 1154 (2005)



Laser-Driven radioisotope generation: what is missing?

- ❖ Selection of medical **radioisotopes that could benefit more** from the laser-driven technology
- ❖ A **complete numerical simulation** of the process, from laser-driven ion acceleration to ion transport and radionuclide generation
- ❖ Analytical modeling to obtain **predictive scaling laws** for different laser facilities and experimental conditions
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Best suited radionuclides for a feasibility study

^{18}F one of the most used (PET), produced via (p,n)...



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FOCUS ON THE STRENGTHS OF THE LASER-DRIVEN TECHNOLOGY

Cost reduction, portability

Versatility



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ULTRASHORT-LIVED ISOTOPES

^{11}C

β^+ PET

Very short $T_{1/2} \sim 20$ min

^{11}B (p,n) ^{11}C

Target: $^{11}\text{B}_2\text{O}_3$



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EMERGING ISOTOPES

^{64}Cu

Odd-odd nuclei:

β^- TRT

β^+ PET

→ THERAGNOSTIC

^{64}Ni (p,n) ^{64}Cu

Target: 100% ^{64}Ni



Best suited radionuclides for a feasibility study

~~¹⁸F~~ one of the most used (PET), produced via (p,n)... But cyclotrons are perfectly optimized for it!

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ULTRASHORT-LIVED ISOTOPES

¹¹C

β⁺ PET

Very short T_{1/2} ~ 20 min

¹¹B (p,n) ¹¹C

Target: ¹¹B₂O₃

Versatility



EMERGING ISOTOPES

⁶⁴Cu

Odd-odd nuclei:

β⁻ TRT

β⁺ PET

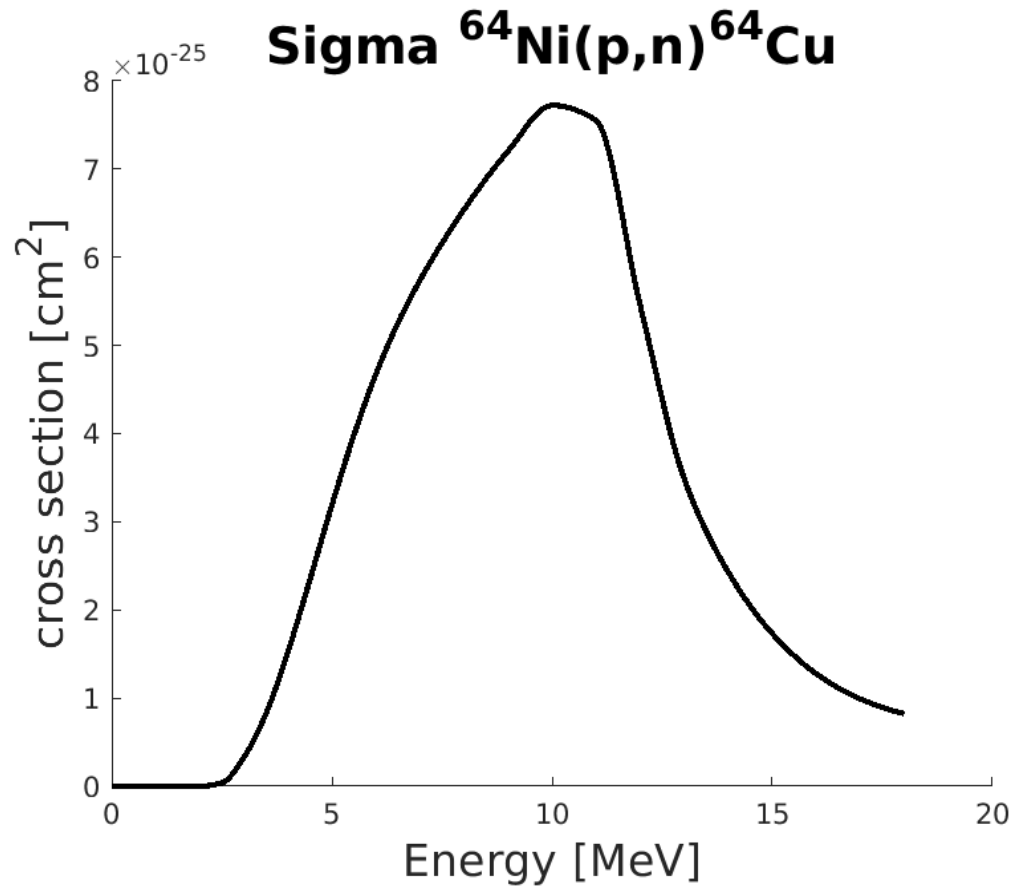
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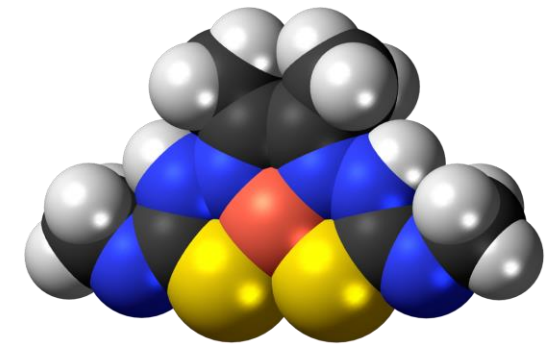
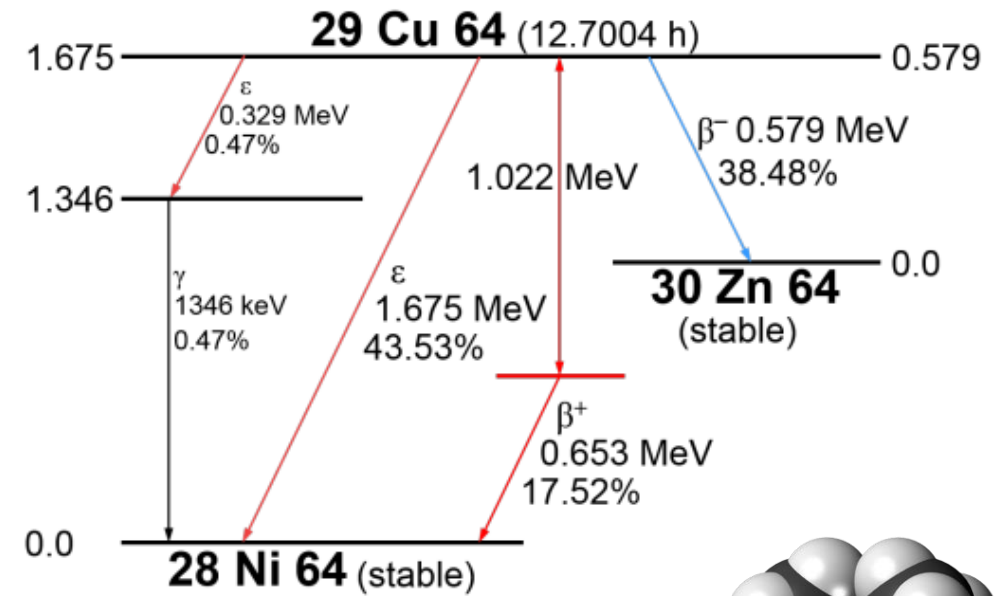
Target: 100% ⁶⁴Ni



^{64}Cu for theragnostics



Reasonably high cross section for proton energy easily **achievable with today's laser** technology



^{64}Cu -ATSM – copper(II)
(diacetyl-bis (N4-methylthiosemicarbazone))

Cyclotron Produced Radionuclides: Emerging Positron Emitters for Medical Applications: ^{64}Cu , IAEA Technical reports 2016

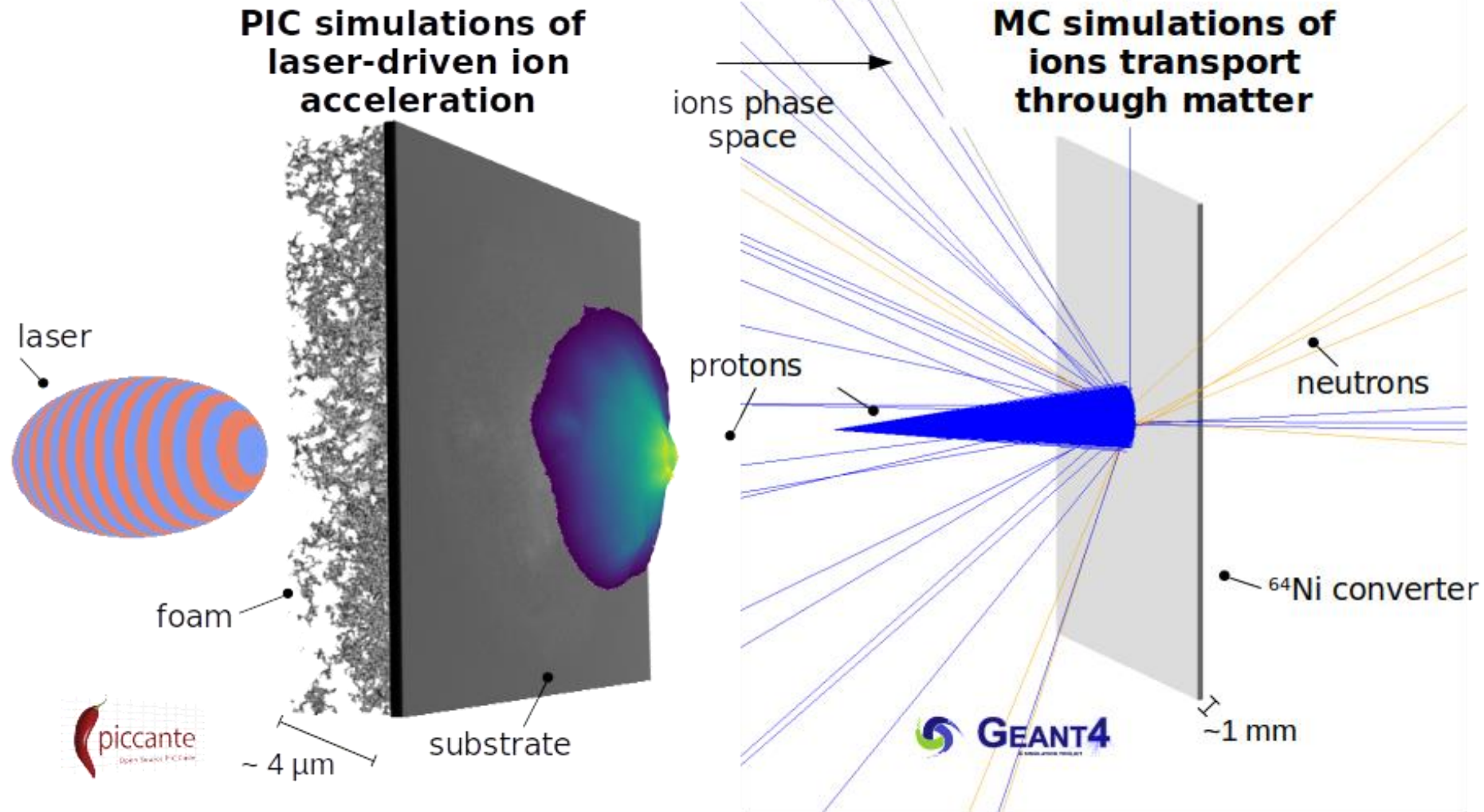


Laser-Driven radioisotope generation: what is missing?

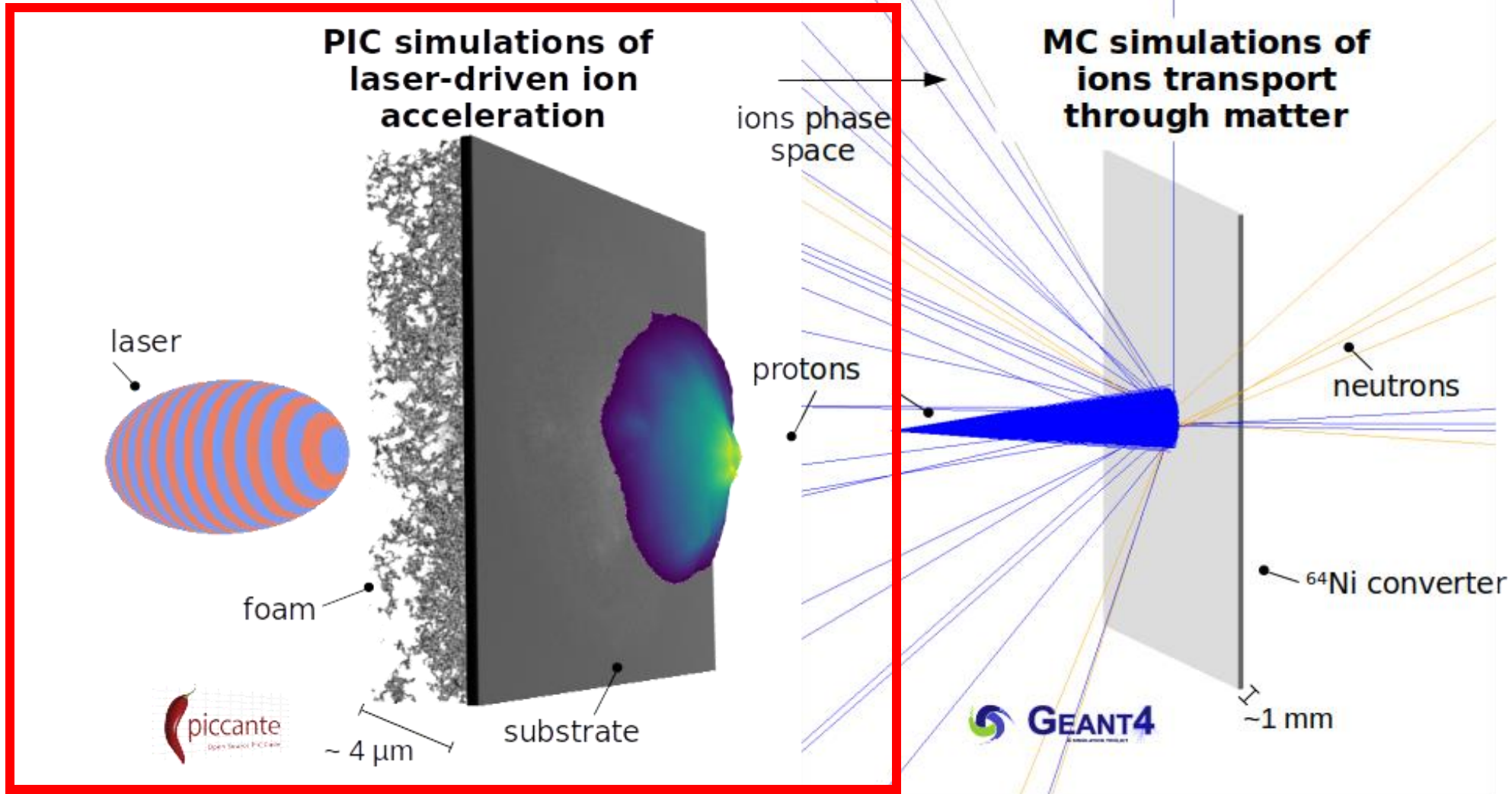
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A complete numerical simulation of the whole process



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Particle-In-Cell simulations

Particle-in-Cell simulations

Simulation setup:

Full 3D PICs

$a_0=16$

Spot size = 5λ

Pulse duration = $15 \lambda/c$

Four target configurations:

 **Simple foil, 0° incidence**

 **Simple foil, 45° incidence**

 **DLT, 0° incidence**

 **DLT, 45° incidence**



Particle-in-Cell simulations

Simulation setup:

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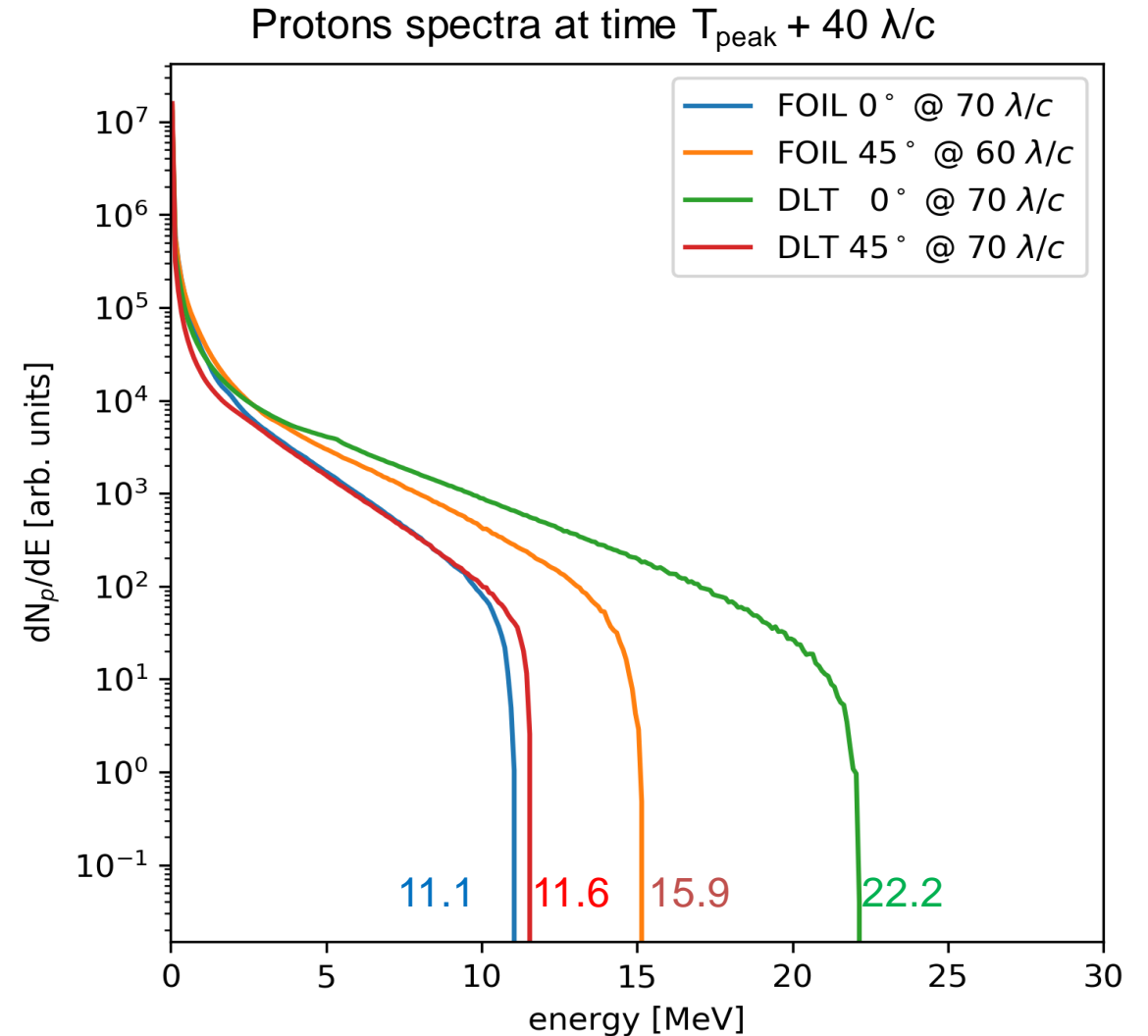
Four target configurations:

☢ Simple foil, 0° incidence

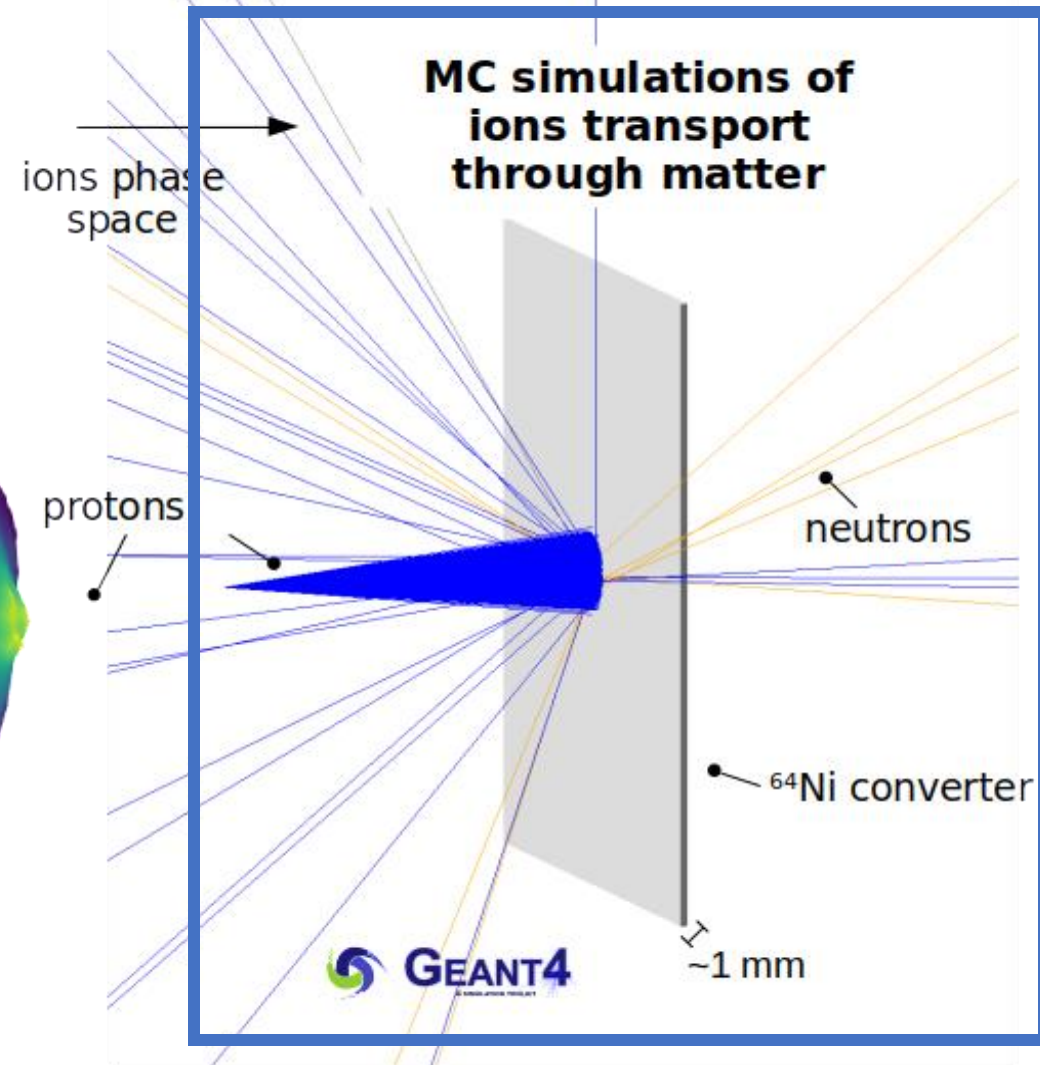
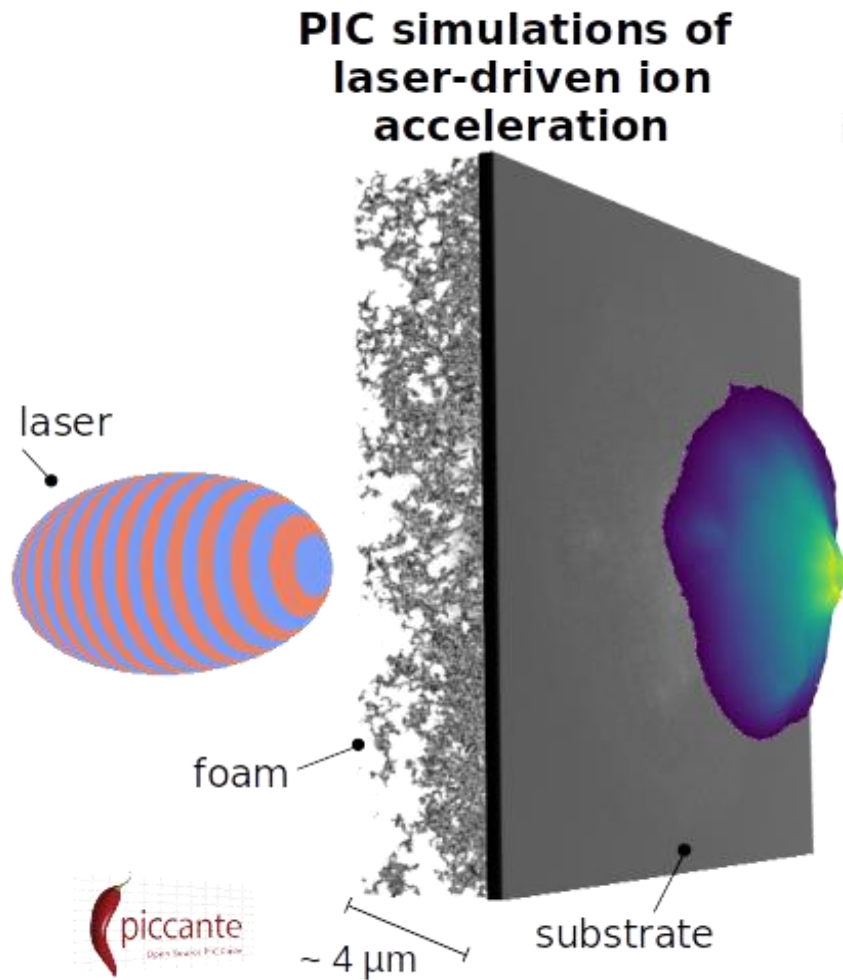
☢ Simple foil, 45° incidence

☢ DLT, 0° incidence

☢ DLT, 45° incidence



A complete numerical simulation of the whole process



Monte Carlo simulations



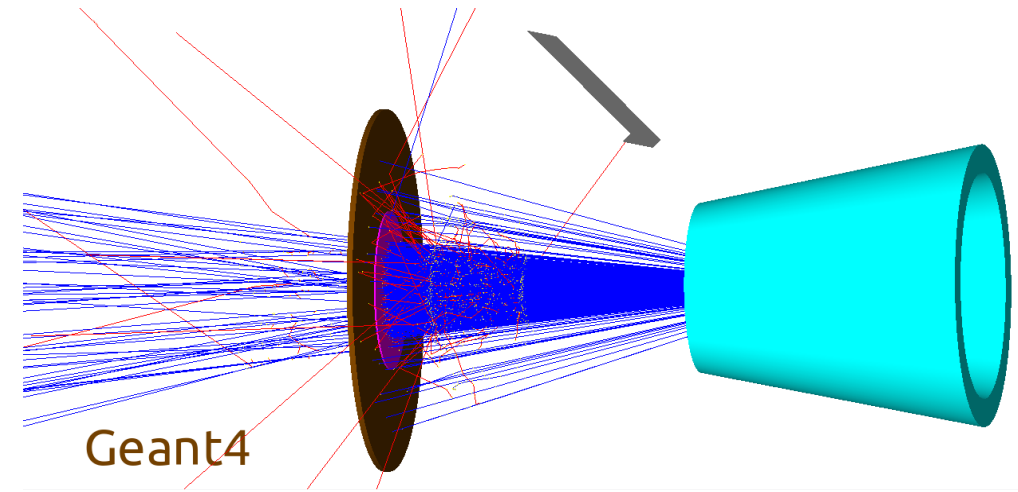
Monte Carlo simulation of proton transport and reaction



(GEometry AND Tracking)

The toolkit allows to:

- ☢ Create a geometrical model \Rightarrow Different shapes
 \Rightarrow Different materials
- ☢ Select a set of particles
- ☢ Physics processes \rightarrow **Physics Lists**



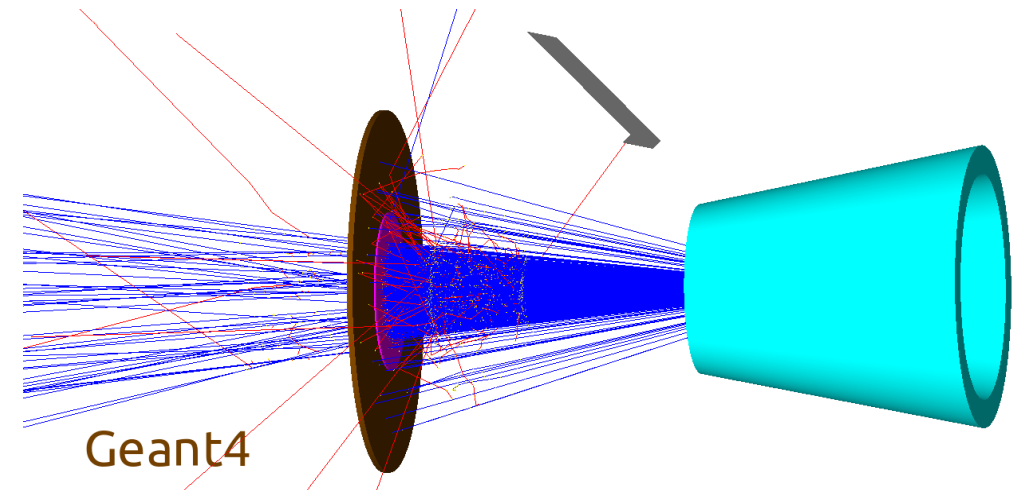
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Setup:

1 mm thick, pure ^{64}Ni target

$4 \cdot 10^6$ proton per run

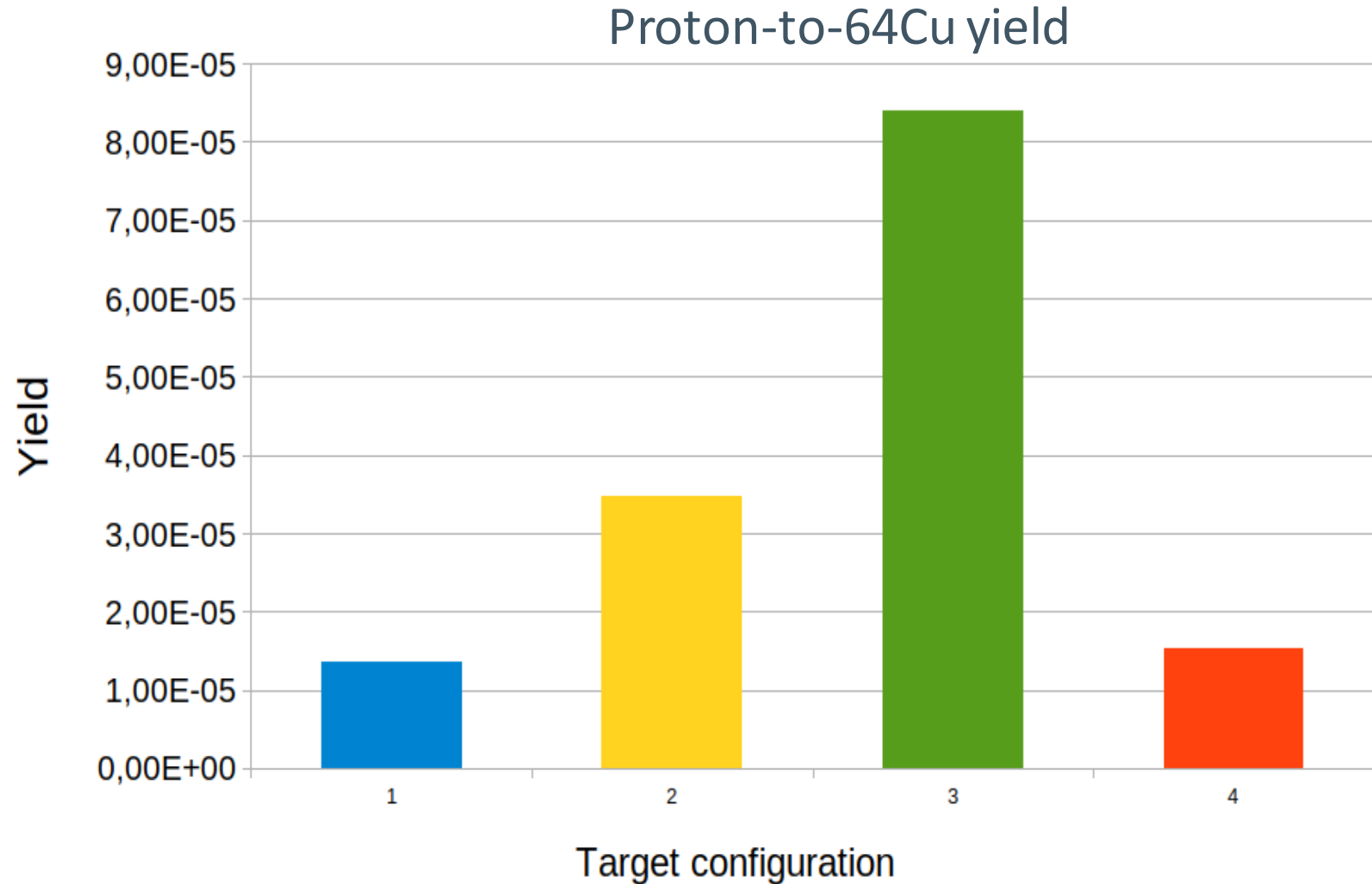
Proton sampled from PIC output spectra

Goal: to determine the proton-to- ^{64}Cu **Yield** (i.e. number of ^{64}Cu per incident proton)



Coupling PIC and Monte Carlo

- Simple foil, 0° incidence
- Simple foil, 45° incidence
- DLT, 0° incidence
- DLT, 45° incidence



Coupling PIC and Monte Carlo

☢ Simple foil, 0° incidence

☢ Simple foil, 45° incidence

☢ DLT, 0° incidence

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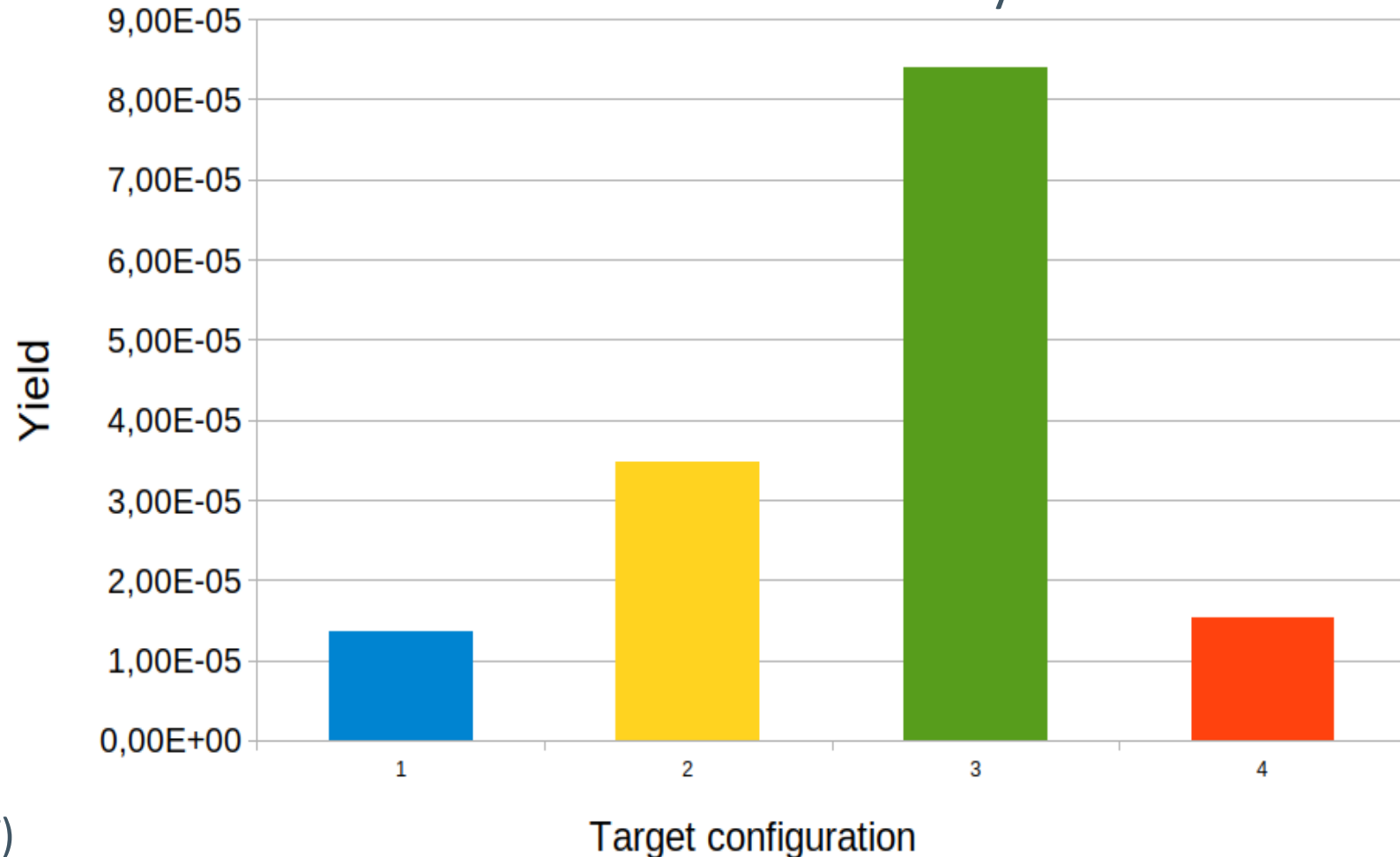
Considering

- 10 Hz rep. Rate,

- 10^{10} proton >1 MeV:

~ **80 MBq activity** (40% of a standar PET)

Proton-to-64Cu yield



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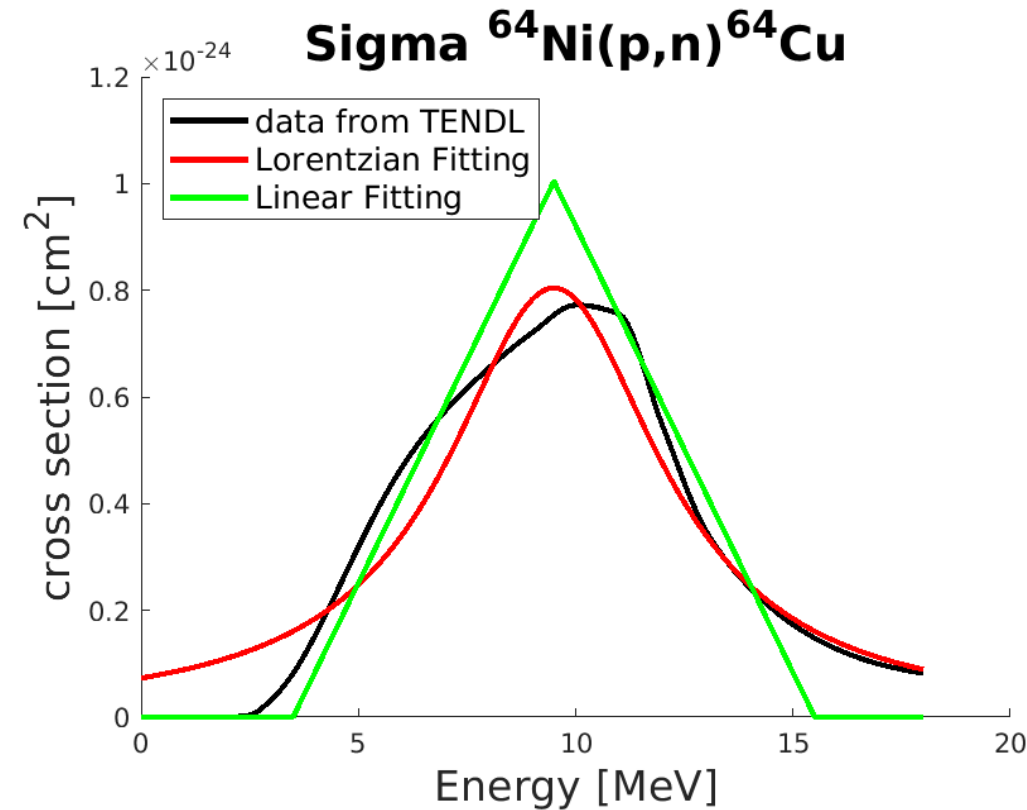
Analytical modeling to obtain predictive scaling laws

$$\frac{dN_{iso}}{dt} \propto \int_0^{E_{co}} f_p(E_i) n_{p,tot} \left(\int_0^{E_i} \frac{\sigma(E_s)}{S(E_s)} dE_s \right) dE_i$$



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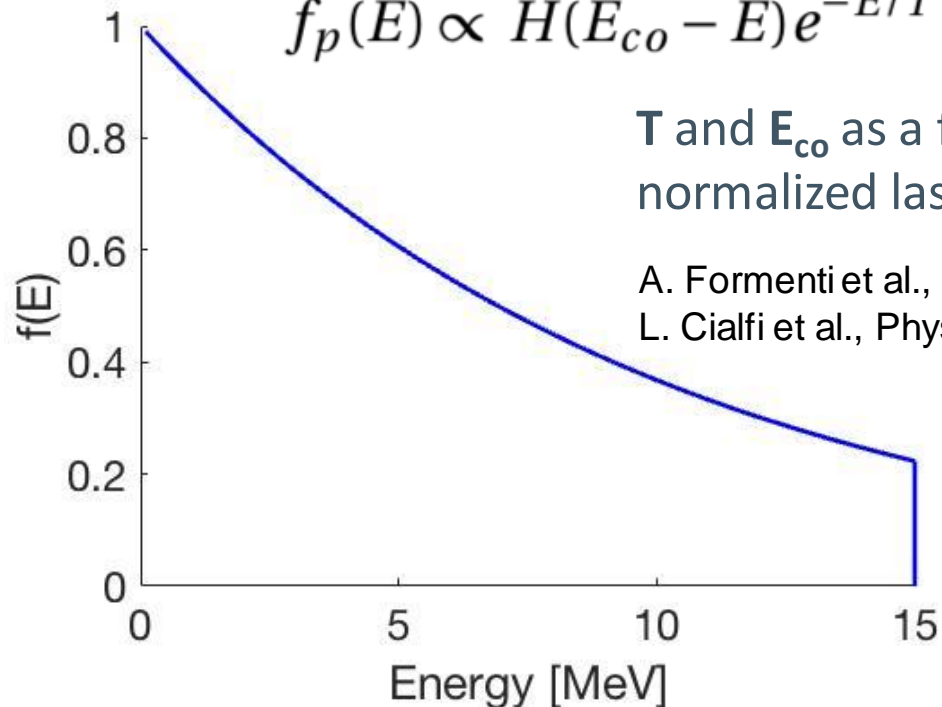
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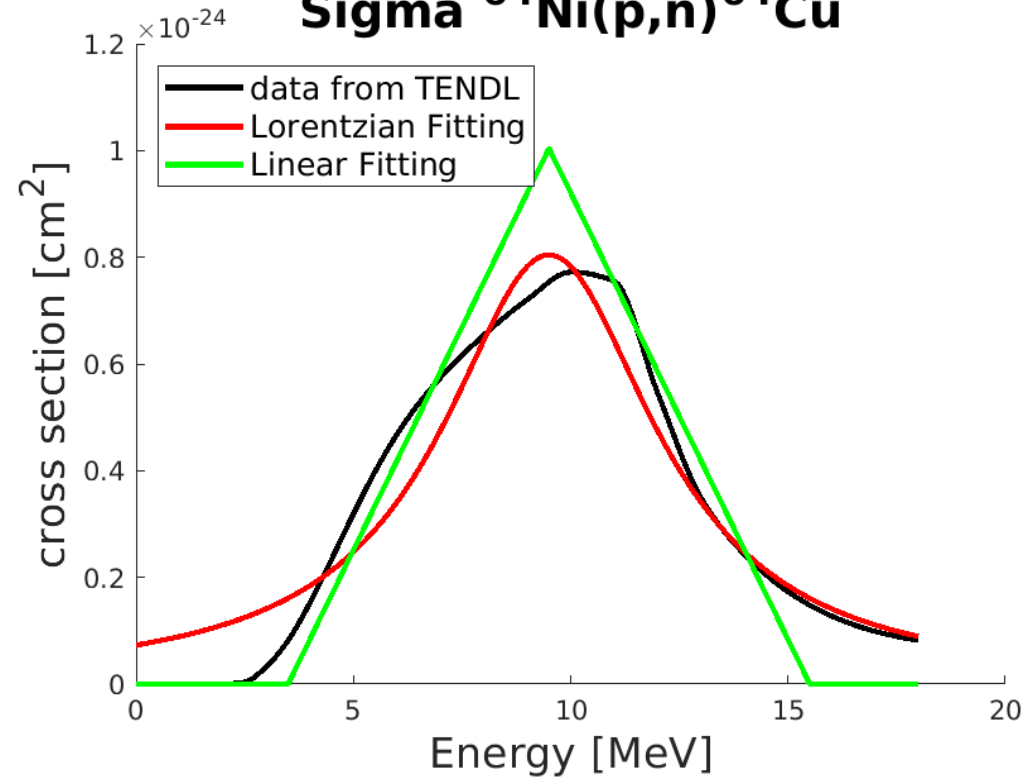
$$f_p(E) \propto H(E_{co} - E) e^{-E/T}$$

T and E_{co} as a function of normalized laser intensity a_0

A. Formenti et al., N. Jour. Physics 22, 053020 (2020)
L. Cialfi et al., Phys. Rev. E 94, 053201 (2016)



Sigma $^{64}\text{Ni}(p,n)^{64}\text{Cu}$



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Thank you for your attention!

